

EXHIBIT 4



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(54) **HUMAN ACTIVITY MONITORING DEVICE**

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7/00; G01P 13/00; G06F 11/00, 11/30, 11/32,
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See application file for complete search history.

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(56) **References Cited**

U.S. PATENT DOCUMENTS

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4,285,041 A 8/1981 Smith
4,578,769 A 3/1986 Frederick
5,446,725 A 8/1995 Ishiwatari
5,446,775 A 8/1995 Wright et al.

(Continued)

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FOREIGN PATENT DOCUMENTS

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JP 2005-309691 A * 11/2005

OTHER PUBLICATIONS

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Jan. 26, 2010, now Pat. No. 7,881,902, which is a
continuation of application No. 11/644,455, filed on
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Cheng, et al, "Periodic Human Motion Description for Sports Video
Databases," Proceedings of the Pattern Recognition, 2004, 5 pages.

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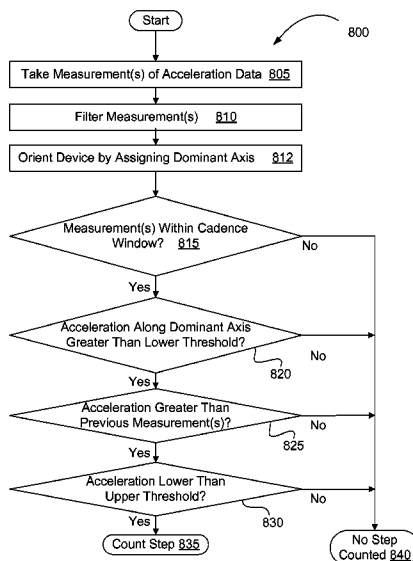
(52) **U.S. Cl.**
USPC **702/160**; 73/1.79; 377/24.2; 702/97;
702/187; 702/189; 708/105; 708/200

(57) **ABSTRACT**

(58) **Field of Classification Search**
USPC 33/700, 701; 73/1.01, 1.37, 1.38, 1.75,
73/1.76, 1.77, 1.78, 1.79, 1.81, 432.1,
73/865.4, 865.8; 377/1, 13, 15, 17, 19, 20,

A method for monitoring human activity using an inertial
sensor includes continuously determining an orientation of
the inertial sensor; assigning a dominant axis, updating the
dominant axis as the orientation of the inertial sensor
changes, and counting periodic human motions by monitor-
ing accelerations relative to the dominant axis.

19 Claims, 9 Drawing Sheets



US 8,712,723 B1

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(56)

References Cited

U.S. PATENT DOCUMENTS

5,485,402 A *	1/1996	Smith et al.	702/160	7,892,080 B1	2/2011	Dahl	
5,583,776 A	12/1996	Levi et al.		7,962,312 B2 *	6/2011	Darley et al.	702/165
5,593,431 A	1/1997	Sheldon		7,987,070 B2 *	7/2011	Kahn et al.	702/160
5,654,619 A	8/1997	Iwashita		8,187,182 B2 *	5/2012	Kahn et al.	600/300
5,778,882 A	7/1998	Raymond et al.		2002/0023654 A1	2/2002	Webb	
5,955,667 A	9/1999	Fyfe		2002/0089425 A1	7/2002	Kubo et al.	
5,976,083 A	11/1999	Richardson et al.		2002/0109600 A1	8/2002	Mault et al.	
6,013,007 A	1/2000	Root et al.		2002/0118121 A1	8/2002	Lehrman et al.	
6,122,595 A	9/2000	Varley et al.		2002/0151810 A1	10/2002	Wong et al.	
6,135,951 A	10/2000	Richardson et al.		2003/0018430 A1	1/2003	Ladetto et al.	
6,145,389 A	11/2000	Ebeling et al.		2003/0048218 A1	3/2003	Milnes et al.	
6,282,496 B1	8/2001	Chowdhary		2003/0083596 A1	5/2003	Kramer et al.	
6,353,449 B1	3/2002	Gregg et al.		2003/0109258 A1	6/2003	Mantyjarvi et al.	
6,369,794 B1	4/2002	Sakurai et al.		2003/0139692 A1	7/2003	Barrey et al.	
6,428,490 B1	8/2002	Kramer et al.		2004/0225467 A1	11/2004	Vock et al.	
6,493,652 B1	12/2002	Ohlenbusch et al.		2004/0236500 A1	11/2004	Choi et al.	
6,496,695 B1	12/2002	Kouji et al.		2005/0033200 A1	2/2005	Soehren et al.	
6,513,381 B2	2/2003	Fyfe et al.		2005/0202934 A1	9/2005	Olrik et al.	
6,522,266 B1	2/2003	Soehren et al.		2005/0210300 A1	9/2005	Song et al.	
6,532,419 B1	3/2003	Begin et al.		2005/0222801 A1	10/2005	Wulff et al.	
6,539,336 B1	3/2003	Vock et al.		2005/0232388 A1	10/2005	Tsuji	
6,611,789 B1	8/2003	Darley		2005/0232404 A1	10/2005	Gaskill	
6,700,499 B2	3/2004	Kubo et al.		2005/0238132 A1	10/2005	Tsuji	
6,771,250 B1	8/2004	Oh		2005/0240375 A1	10/2005	Sugai	
6,786,877 B2	9/2004	Foxlin		2005/0245988 A1	11/2005	Miesel	
6,790,178 B1	9/2004	Mault et al.		2005/0248718 A1	11/2005	Howell et al.	
6,813,582 B2	11/2004	Levi et al.		2006/0020177 A1	1/2006	Seo et al.	
6,823,036 B1	11/2004	Chen		2006/0063980 A1	3/2006	Hwang et al.	
6,826,477 B2	11/2004	Ladetto et al.		2006/0064276 A1	3/2006	Ren et al.	
6,836,744 B1	12/2004	Asphahani et al.		2006/0100546 A1	5/2006	Silk	
6,881,191 B2	4/2005	Oakley et al.		2006/0136173 A1	6/2006	Case, Jr. et al.	
6,885,971 B2	4/2005	Vock et al.		2006/0149516 A1	7/2006	Bond et al.	
6,898,550 B1	5/2005	Blackadar et al.		2006/0161377 A1	7/2006	Rakkola et al.	
6,928,382 B2	8/2005	Hong et al.		2006/0167387 A1	7/2006	Buchholz et al.	
6,941,239 B2	9/2005	Unuma et al.		2006/0174685 A1 *	8/2006	Skvortsov et al.	73/1.37
6,959,259 B2	10/2005	Vock et al.		2006/0206258 A1	9/2006	Brooks	
6,975,959 B2	12/2005	Dietrich et al.		2006/0223547 A1	10/2006	Chin et al.	
7,010,332 B1	3/2006	Irvin et al.		2006/0259268 A1	11/2006	Vock et al.	
7,054,784 B2	5/2006	Flentov et al.		2006/0284979 A1	12/2006	Clarkson	
7,057,551 B1	6/2006	Vogt		2006/0288781 A1	12/2006	Daumer et al.	
7,072,789 B2	7/2006	Vock et al.		2007/0038364 A1	2/2007	Lee et al.	
7,092,846 B2	8/2006	Vock et al.		2007/0061105 A1	3/2007	Darley et al.	
7,148,797 B2	12/2006	Albert		2007/0063850 A1	3/2007	Devaul et al.	
7,158,912 B2	1/2007	Vock et al.		2007/0067094 A1	3/2007	Park et al.	
7,169,084 B2	1/2007	Tsuji		2007/0073482 A1	3/2007	Churchill et al.	
7,171,331 B2	1/2007	Vock et al.		2007/0082789 A1	4/2007	Nissila et al.	
7,177,684 B1	2/2007	Kroll et al.		2007/0125852 A1	6/2007	Rosenberg	
7,200,517 B2	4/2007	Darley et al.		2007/0130582 A1	6/2007	Chang et al.	
7,212,943 B2	5/2007	Aoshima et al.		2007/0142715 A1	6/2007	Banet et al.	
7,220,220 B2	5/2007	Stubbs et al.		2007/0143068 A1 *	6/2007	Pasolini et al.	702/160
7,297,088 B2	11/2007	Tsuji		2007/0145680 A1	6/2007	Rosenberg	
7,305,323 B2 *	12/2007	Skvortsov et al.	702/160	2007/0150136 A1	6/2007	Doll et al.	
7,328,611 B2	2/2008	Klees et al.		2007/0208531 A1	9/2007	Darley et al.	
7,334,472 B2	2/2008	Seo et al.		2007/0213126 A1	9/2007	Deutsch et al.	
7,353,112 B2	4/2008	Choi et al.		2007/0250261 A1	10/2007	Soehren	
7,387,611 B2	6/2008	Inoue et al.		2007/0259716 A1	11/2007	Mattice et al.	
7,428,471 B2 *	9/2008	Darley et al.	702/182	2007/0259717 A1	11/2007	Mattice et al.	
7,451,056 B2	11/2008	Flentov et al.		2007/0260418 A1	11/2007	Ladetto et al.	
7,457,719 B1	11/2008	Kahn et al.		2007/0260482 A1	11/2007	Nurmela et al.	
7,463,997 B2 *	12/2008	Pasolini et al.	702/160	2008/0171918 A1	7/2008	Teller et al.	
7,467,060 B2	12/2008	Kulach et al.		2008/0243432 A1 *	10/2008	Kato et al.	702/160
7,512,515 B2	3/2009	Vock et al.		2009/0043531 A1	2/2009	Kahn et al.	
7,526,402 B2	4/2009	Tananhaus et al.		2009/0047645 A1	2/2009	Dibenedetto et al.	
7,608,050 B2	10/2009	Shugg		2009/0124348 A1	5/2009	Yoseloff et al.	
7,617,071 B2 *	11/2009	Darley et al.	702/165	2009/0213002 A1	8/2009	Rani et al.	
7,640,134 B2 *	12/2009	Park et al.	702/141	2009/0234614 A1	9/2009	Kahn et al.	
7,640,804 B2	1/2010	Daumer et al.		2009/0319221 A1	12/2009	Kahn et al.	
7,647,196 B2	1/2010	Kahn et al.		2010/0056872 A1	3/2010	Kahn et al.	
7,653,508 B1	1/2010	Kahn et al.		2010/0057398 A1	3/2010	Darley et al.	
7,752,011 B2	7/2010	Niva et al.					
7,753,861 B1	7/2010	Kahn et al.					
7,774,156 B2	8/2010	Niva et al.					
7,788,059 B1 *	8/2010	Kahn et al.	702/141				
7,857,772 B2	12/2010	Bouvier et al.					
7,881,902 B1 *	2/2011	Kahn et al.	702/160				

OTHER PUBLICATIONS

Heart Rate Monitors, .suunto.com/suunto/Worlds/main/world_article_product_no_ATL.jsp?CONTENT%3C%3Ecnt_id=10134198676968765&FOLDER%3C%3Efolder_d=9852723697225397&ASSORTMENT%3C%3East_id=1408474395903593&bmUID=1174532640618speed>, Apr. 4, 2007, 1 page.

US 8,712,723 B1

Page 3

(56)

References Cited

OTHER PUBLICATIONS

Jones, L., et al., "Wireless Physiological Sensor System for Ambulatory Use," ieeexplore.ieee.org/xpl/freeabs_all.jsp?tp=&arnumber=1612917&isnumber=33861>, Apr. 3-5, 2006.

"Sensor Fusion," u-dynamics.com>, accessed Aug. 29, 2008, 2 pages.

Sinha, Alex, "Heart Monitoring Training," marathonguide.com/training/articles/HeartMonitorTraining.cfm>, Apr. 4, 2007, 5 pages.

Wang, Shu, et al., "Location Based Services for Mobiles: Technologies and Standards, LG Electronics MobileComm," IEEE ICC 2008, Beijing, pp. 1-66 (part 1 of 3).

Wang, Shu, et al., "Location Based Services for Mobiles: Technologies and Standards, LG Electronics MobileComm," IEEE ICC 2008, Beijing, pp. 67-92 (part 2 of 3).

Wang, Shu, et al., "Location Based Services for Mobiles: Technologies and Standards, LG Electronics MobileComm," IEEE ICC 2008, Beijing, pp. 93-123 (part 3 of 3).

Weckesser, P., et al., "Multiple Sensorprocessing for High-Precision Navigation and Environmental Modeling with a Mobile Robot," IEEE, 1995, pp. 453-458.

Yoo, Chang-Sun, et al., "Low Cost GPS/INS Sensor Fusion System for UAV Navigation," IEEE, 2003, 9 pages.

Anderson, Ian, et al., "Shakra: Tracking and Sharing Daily Activity Levels with Unaugmented Mobile Phones," Mobile Netw Appl, Aug. 3, 2007, pp. 185-199.

Aylward, Ryan, et al., "Senseable: A Wireless, Compact, Multi-User Sensor System for Interactive Dance," International Conference on New Interfaces for Musical Expression (NIME06), Jun. 4-8, 2006, pp. 134-139.

Baca, Arnold, et al., "Rapid Feedback Systems for Elite Sports Training," IEEE Pervasive Computing, Oct.-Dec. 2006, pp. 70-76.

Bakhru, Kesh, "A Seamless Tracking Solution for Indoor and Outdoor Position Location," IEEE 16th International Symposium on Personal, Indoor, and Mobile Radio Communications, 2005, pp. 2029-2033.

Bliley, Kara E., et al., "A Miniaturized Low Power Personal Motion Analysis Logger Utilizing MEMS Accelerometers and Low Power Microcontroller," IEEE EMBS Special Topic Conference on Microtechnologies in Medicine and Biology, May 12-15, 2005, pp. 92-93.

Fang, Lei, et al., "Design of a Wireless Assisted Pedestrian Dead Reckoning System—The NavMote Experience," IEEE Transactions on Instrumentation and Measurement, vol. 54, No. 6, Dec. 2005, pp. 2342-2358.

Healey, Jennifer, et al., "Wearable Wellness Monitoring Using ECG and Accelerometer Data," IEEE Int. Symposium on Wearable Computers (ISWC'05), 2005, 2 pages.

Hemmes, Jeffrey, et al., "Lessons Learned Building TeamTrak: An Urban/Outdoor Mobile Testbed," 2007 IEEE Int. Conf. on Wireless Algorithms, Aug. 1-3, 2007, pp. 219-224.

Jovanov, Emil, et al., "A Wireless Body Area Network of Intelligent Motion Sensors for Computer Assisted Physical Rehabilitation," Journal of NeuroEngineering and Rehabilitation, Mar. 2005, 10 pages.

Kalpaxis, Alex, "Wireless Temporal-Spatial Human Mobility Analysis Using Real-Time Three Dimensional Acceleration Data," IEEE Intl. Multi-Conf. on Computing in Global IT (ICCGI'07), 2007, 7 pages.

Milenkovic, Milena, et al., "An Accelerometer-Based Physical Rehabilitation System," IEEE SouthEastern Symposium on System Theory, 2002, pp. 57-60.

Otto, Chris, et al., "System Architecture of a Wireless Body Area Sensor Network for Ubiquitous Health Monitoring," Journal of Mobile Multimedia, vol. 1, No. 4, 2006, pp. 307-326.

Park, Chulsung, et al., "Eco: An Ultra-Compact Low-Power Wireless Sensor Node for Real-Time Motion Monitoring," IEEE Int. Symp. on Information Processing in Sensor Networks, 2005, pp. 398-403.

Shen, Chien-Lung, et al., "Wearable Band Using a Fabric-Based Sensor for Exercise ECG Monitoring," IEEE Int. Symp. on Wearable Computers, 2006, 2 pages.

Tapia, Emmanuel Munguia, et al., "Real-Time Recognition of Physical Activities and Their Intensities Using Wireless Accelerometers and a Heart Rate Monitor," IEEE Cont. on Wearable Computers, Oct. 2007, 4 pages.

Wixted, Andrew J., et al., "Measurement of Energy Expenditure in Elite Athletes Using MEMS-Based Triaxial Accelerometers," IEEE Sensors Journal, vol. 7, No. 4, Apr. 2007, pp. 481-488.

Wu, Winston H., et al., "Context-Aware Sensing of Physiological Signals," IEEE Int. Conf. on Engineering for Medicine and Biology, Aug. 23-26, 2007, pp. 5271-5275.

Bourzac, Katherine "Wearable Health Reports," Technology Review, Feb. 28, 2006, techreview.com/printer_friendly_article.aspx?id=16431, Mar. 22, 2007, 3 pages.

Dao, Ricardo, "Inclination Sensing with Thermal Accelerometers", MEMSIC, May 2002, 3 pages.

Lee, Seon-Woo, et al., "Recognition of Walking Behaviors for Pedestrian Navigation," ATR Media Integration & Communications Research Laboratories, Kyoto, Japan, 4 pages.

Margaria, Rodolfo, "Biomechanics and Energetics of Muscular Exercise", Chapter 3, pp. 105-125, Oxford: Clarendon Press 1976.

Mizell, David, "Using Gravity to Estimate Accelerometer Orientation", Seventh IEEE International Symposium on Wearable Computers, 2003, 2 pages.

Ormonet, D., et al., "Learning and Tracking Cyclic Human Motion," Encyclopedia of Library and Information Science, vol. 53, supplement 16, 2001, 7 pages.

PCT International Search Report and Written Opinion for International Application No. PCT/US2008/072537, mailed Oct. 22, 2008, 10 pages.

PCT International Search Report and Written Opinion for International Application No. PCT/US2009/48523, mailed Aug. 27, 2009, 8 pages.

Weinberg, Harvey, "MEMS Motion Sensors Boost Handset Reliability" Jun. 2006, mwrf.com/Articles/Print.cfm?ArticleID=12740, Feb. 21, 2007, 4 pages.

* cited by examiner

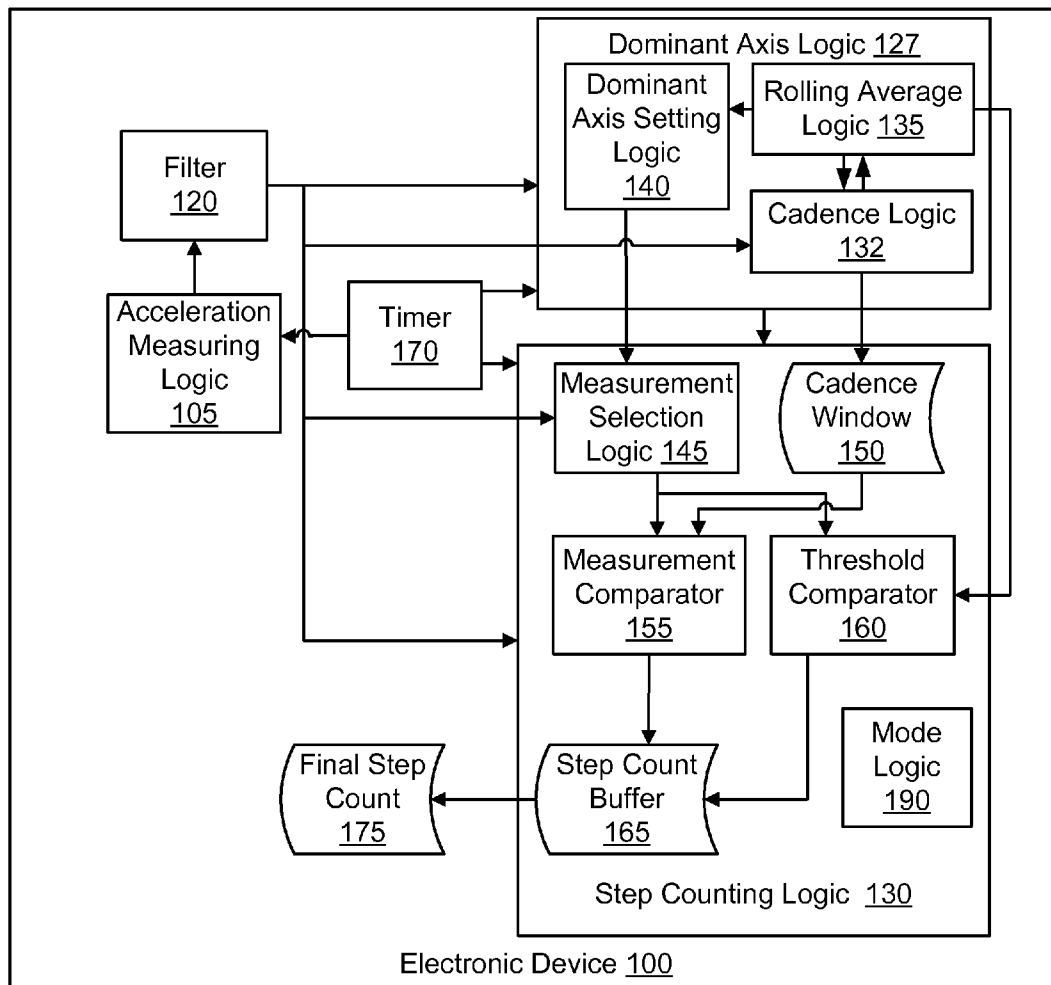


Figure 1

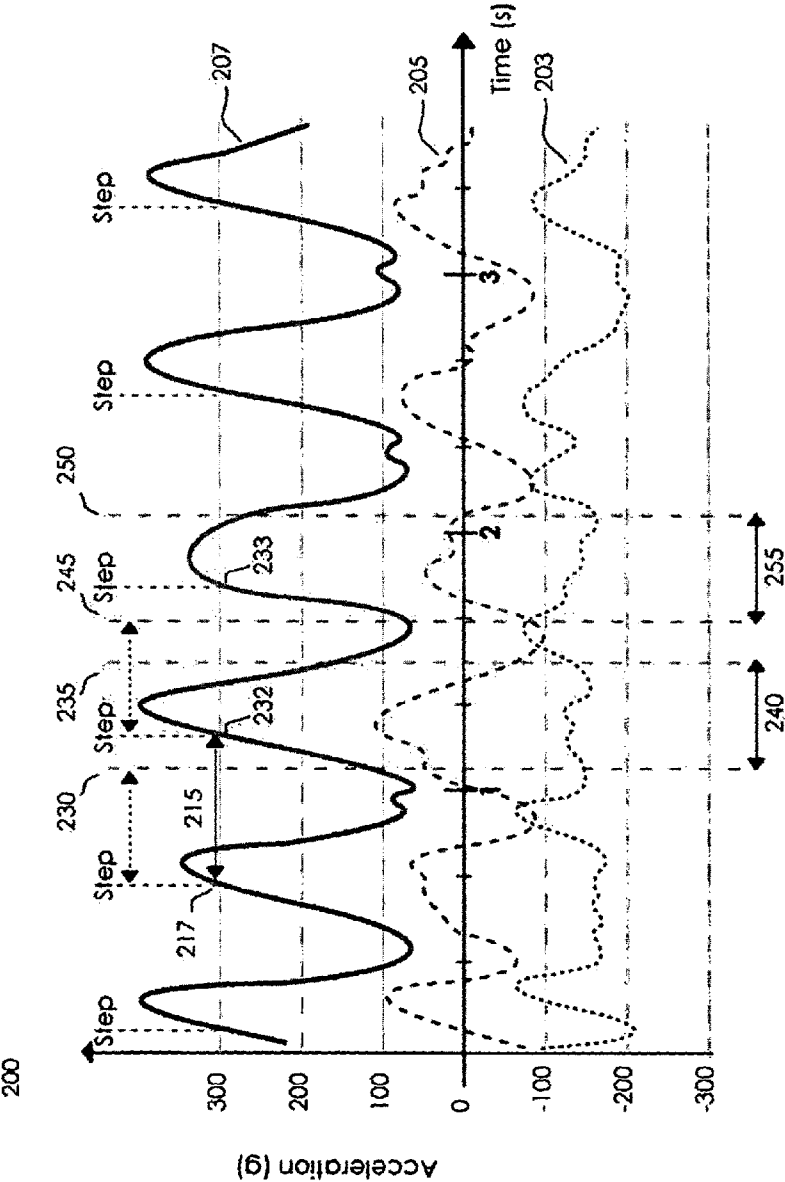


Figure 2

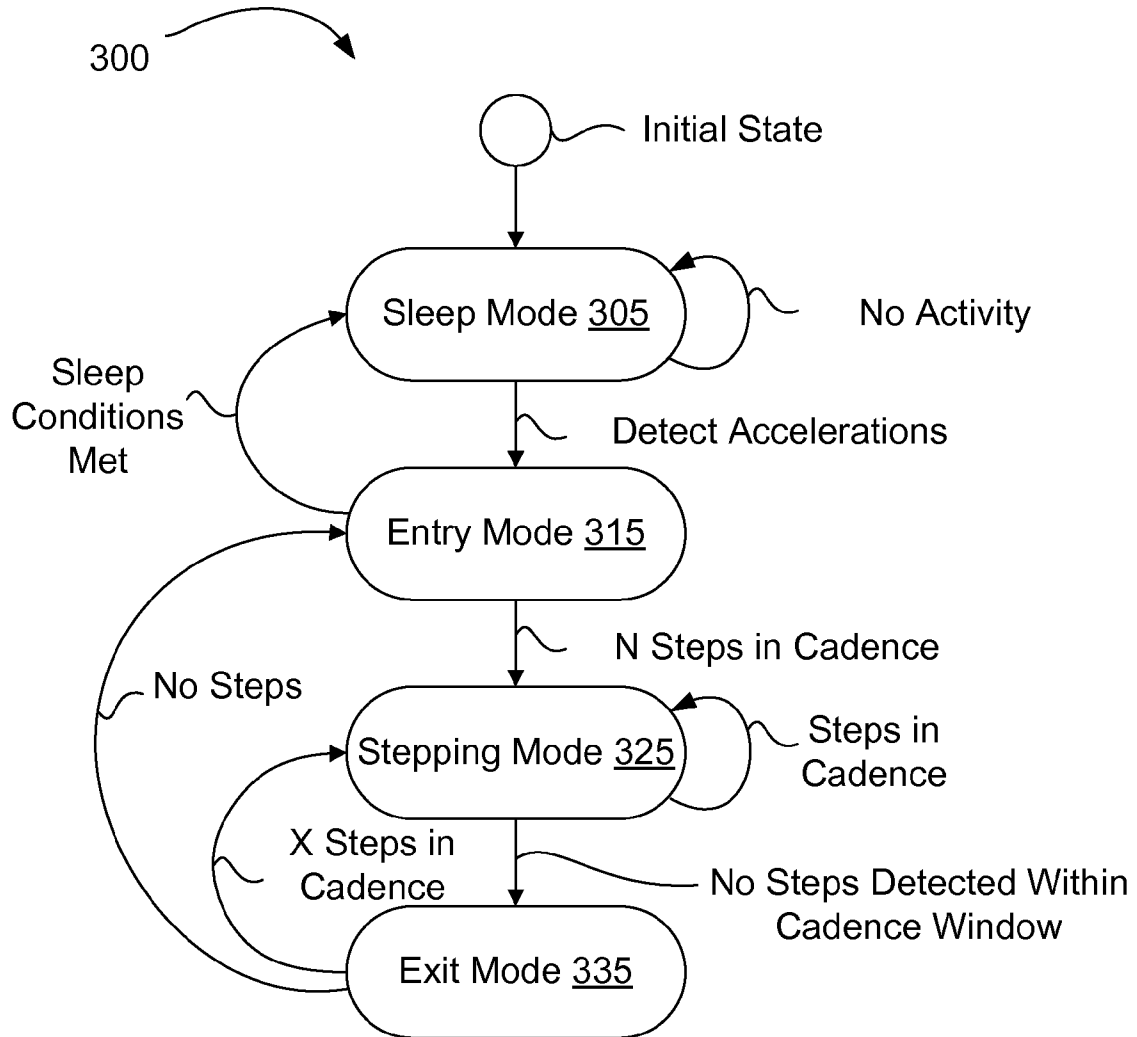


Figure 3

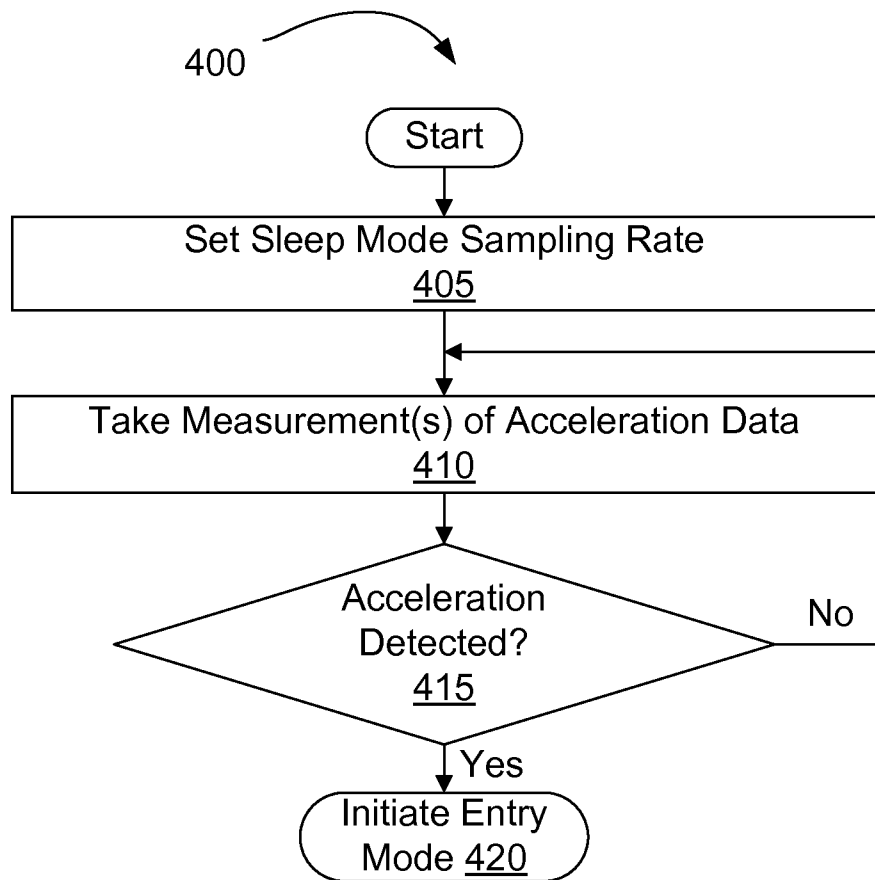


Figure 4

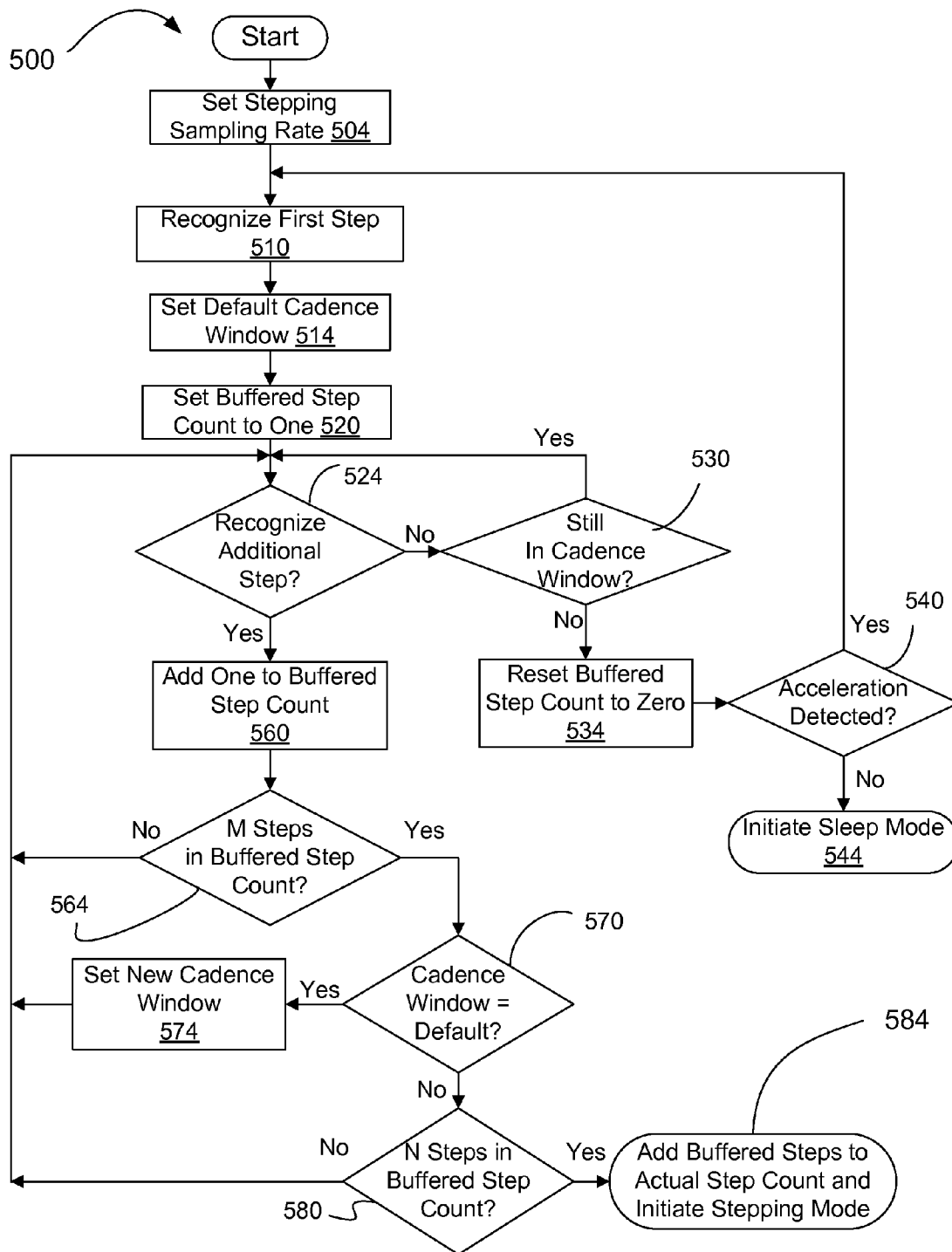


Figure 5

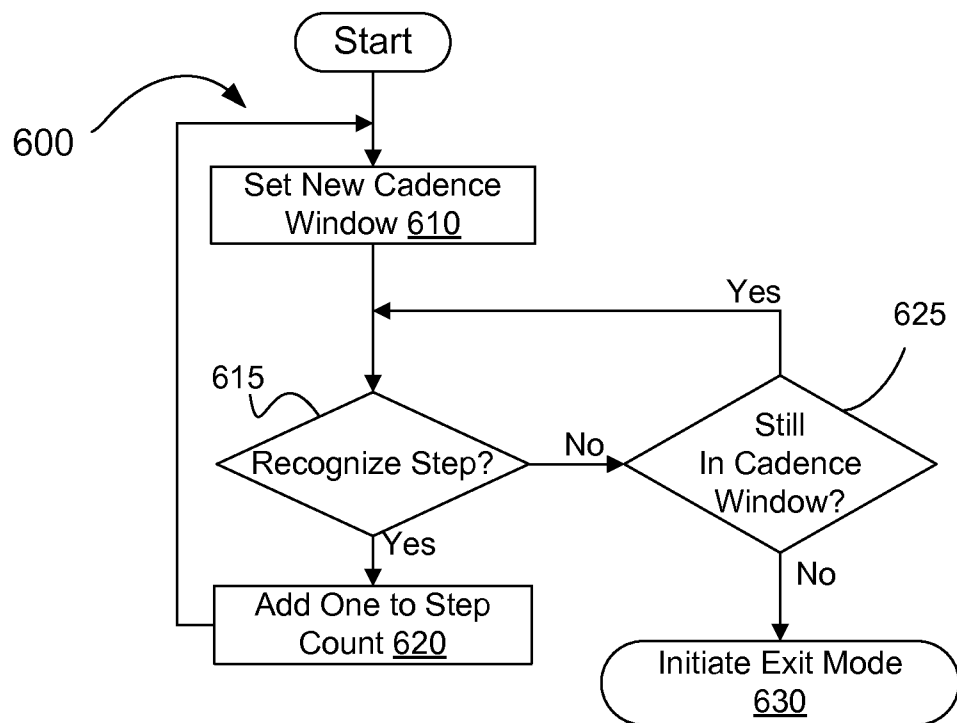


Figure 6

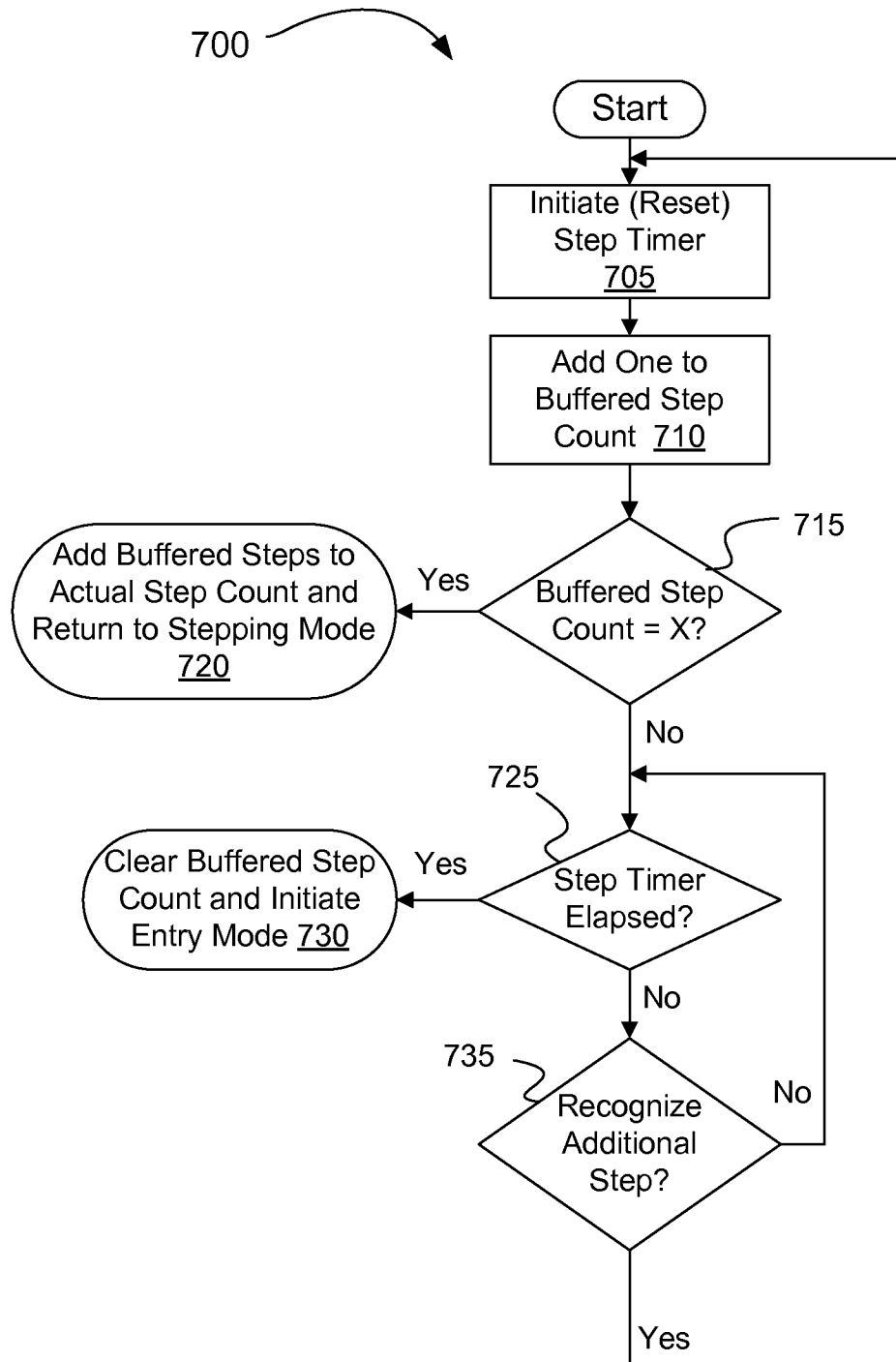


Figure 7

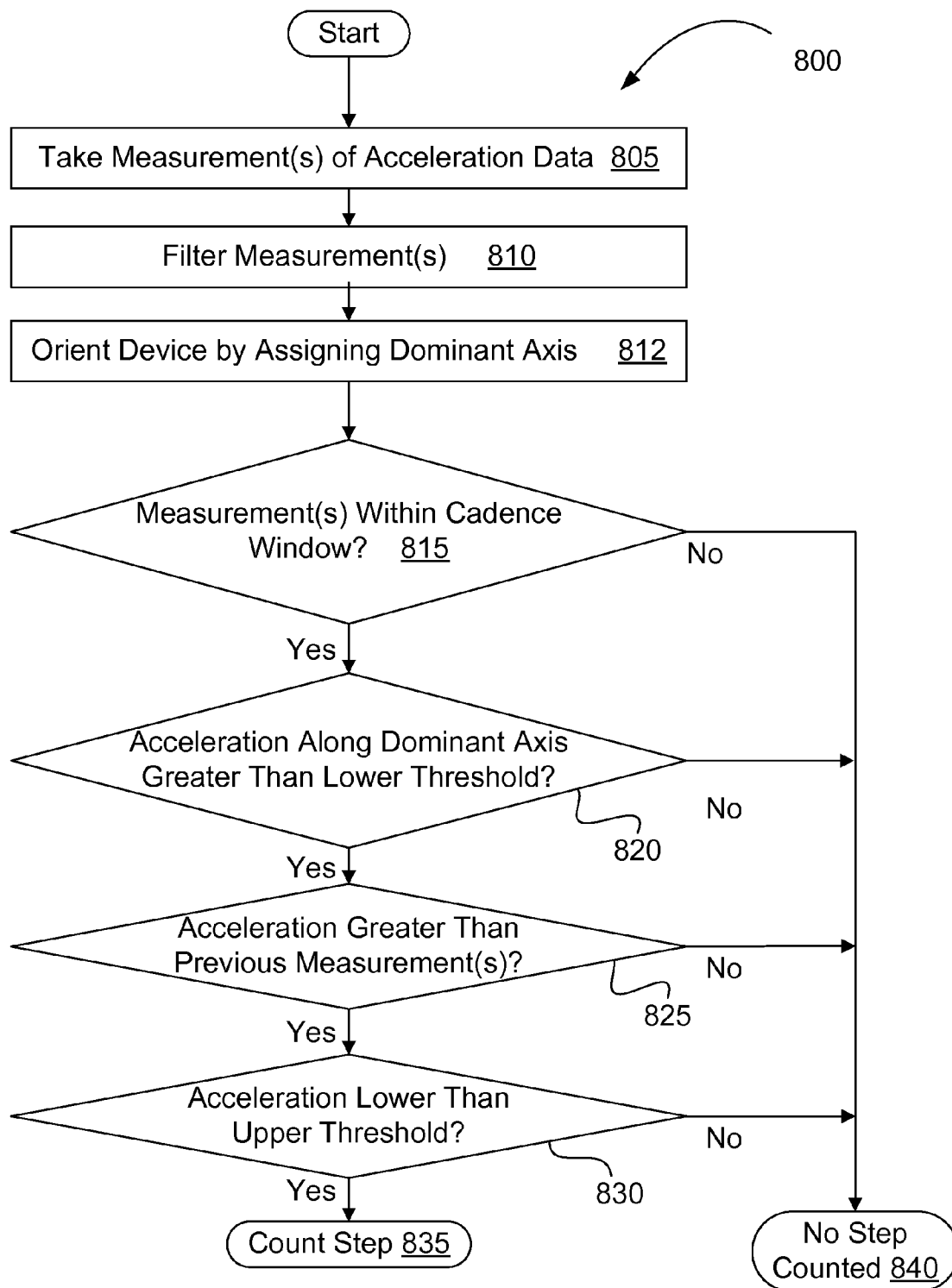


Figure 8

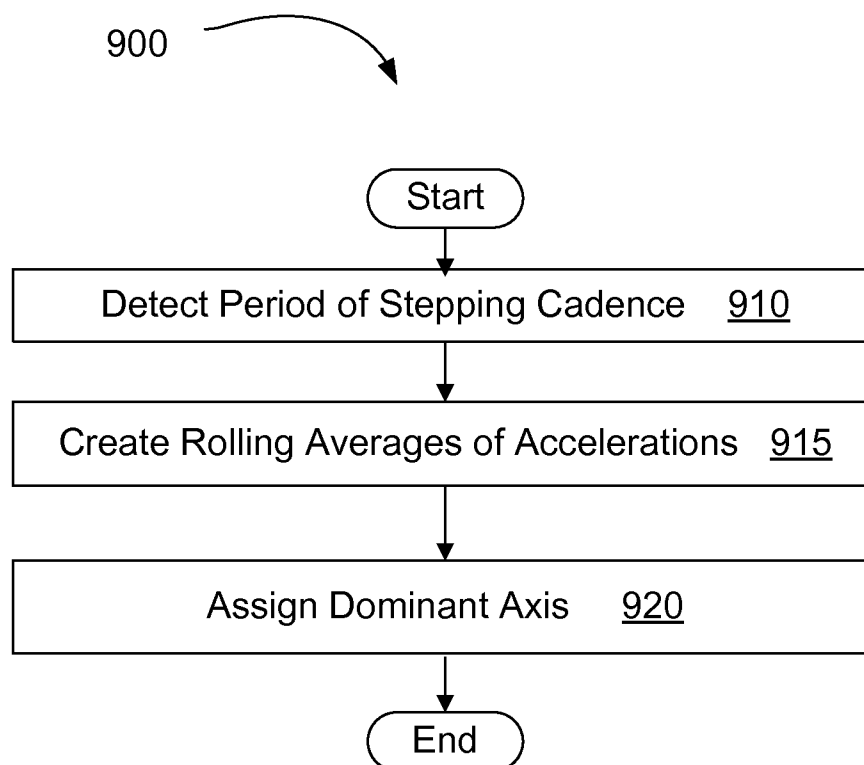


Figure 9

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HUMAN ACTIVITY MONITORING DEVICE

The present patent application is a continuation of U.S. application Ser. No. 12/694,135, filed on Jan. 26, 2010, now U.S. Pat. No. 7,881,902, issued on Feb. 1, 2011; which is a continuation of U.S. application Ser. No. 11/644,455, filed on Dec. 22, 2006, now U.S. Pat. No. 7,653,508, issued on Jan. 26, 2010.

FIELD OF THE INVENTION

This invention relates to a method of monitoring human activity, and more particularly to counting periodic human motions such as steps.

BACKGROUND

The development of Micro-Electro-Mechanical Systems (MEMS) technology has enabled manufacturers to produce inertial sensors (e.g., accelerometers) of sufficient size, cost, and power consumption to fit into portable electronic devices. Such inertial sensors can be found in a limited number of commercial electronic devices such as cellular phones, portable music players, pedometers, game controllers, and portable computers.

Step counting devices are used to monitor an individual's daily activity by keeping track of the number of steps that he or she takes. Generally, step counting devices that utilize an inertial sensor to measure motion to detect steps require the user to first position the device in a limited set of orientations. In some devices, the required orientations are dictated to the user by the device. In other devices, the beginning orientation is not critical, so long as this orientation can be maintained.

Step counting devices are often confused by motion noise experienced by the device throughout a user's daily routine. This noise causes false steps to be measured and actual steps to be missed in conventional step counting devices. Conventional step counting devices also fail to accurately measure steps for individuals who walk at a slow pace. Such step counting devices can fail to operate for seniors and others walking at a slow pace.

BRIEF DESCRIPTION OF THE DRAWINGS

The present invention is illustrated by way of example, and not by way of limitation, and can be more fully understood with reference to the following detailed description when considered in connection with the following figures:

FIG. 1 is a block diagram illustrating one embodiment of an electronic device;

FIG. 2 illustrates an exemplary cadence of motion graph that measures time versus acceleration, in accordance with one embodiment of the present invention;

FIG. 3 shows a state diagram for the behavior of a system of monitoring human activity using an inertial sensor, in accordance with one embodiment of the present invention;

FIG. 4 illustrates a flow diagram for a method of operating an electronic device in sleep mode, in accordance with one embodiment of the present invention;

FIG. 5 illustrates a flow diagram for a method of operating an electronic device in entry mode, in accordance with one embodiment of the present invention;

FIG. 6 illustrates a flow diagram for a method of operating an electronic device in stepping mode, in accordance with one embodiment of the present invention;

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FIG. 7 illustrates a flow diagram for a method of operating an electronic device in exit mode, in accordance with one embodiment of the present invention;

FIG. 8 illustrates a flow diagram for a method of recognizing a step in accordance with one embodiment of the present invention, in accordance with one embodiment of the present invention; and

FIG. 9 illustrates a flow diagram for a method of orienting an inertial sensor, in accordance with one embodiment of the present invention.

DETAILED DESCRIPTION

Embodiments of the present invention are designed to monitor human activity using an inertial sensor. In one embodiment, a dominant axis is assigned after determining an orientation of an inertial sensor. The orientation of the inertial sensor is continuously determined, and the dominant axis is updated as the orientation of the inertial sensor changes. In one embodiment, periodic human motions are counted by monitoring accelerations relative to the dominant axis.

FIG. 1 is a block diagram illustrating an electronic device 100, in accordance with one embodiment of the present invention. The electronic device 100 in one embodiment comprises an acceleration measuring logic 105, a filter 120, a dominant axis logic 127, a step counting logic 130, a timer 170, and a final step count 175. In one embodiment, the electronic device 100 is a portable electronic device that includes one or more inertial sensors. The inertial sensors may measure accelerations along a single axis or multiple axes. The inertial sensors may measure linear as well as rotational (angular) accelerations. The electronic device 100 may be used to count steps or other periodic human motions. Steps may be accurately counted regardless of the placement and/or orientation of the device on a user. Steps may be accurately counted whether the electronic device 100 maintains a fixed orientation or changes orientation during operation. The electronic device 100 may be carried in a backpack, pocket, purse, hand, or elsewhere, and accurate steps may still be counted.

The acceleration measuring logic 105 measures acceleration data at a sampling rate. The sampling rate may be fixed or variable. In one embodiment, the acceleration measuring logic 105 receives a timing signal from the timer 170 in order to take measurements at the sampling rate. The acceleration measuring logic 105 may be an inertial sensor.

In one embodiment, measurement data is processed by the filter 120 to remove noise. The filter 120 may be implemented in hardware, software, or both hardware and software. The filter 120 may include a high pass filter, a low pass filter, a bandpass filter, a bandstop filter and/or additional filters. The filter 120 may include a digital filter and/or an analog filter. In one embodiment, a hardware digital filter includes at least one of a finite impulse response (FIR) filter and an infinite impulse response (IIR) filter. In one embodiment, an N-tap hardware digital FIR filter is used. The use of a hardware FIR filter may reduce power consumption by reducing and/or eliminating software digital filtering.

In one embodiment, the filter 120 includes multiple filters, and a determination of which filters to apply to the measurement data is made based upon an operating mode of the electronic device 100. In one embodiment, the selection of which filters to use is determined by the type of user activity detected. For example, a low pass filter may be used to remove high frequency noise that would interfere with step counting when a user is walking. In contrast, a high pass filter may be used when quick motions are to be monitored.

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Filtered measurement data may be passed on to the dominant axis logic 127 and the step counting logic 130. In one embodiment, the dominant axis logic 127 includes a cadence logic 132, a rolling average logic 135, and a dominant axis setting logic 140. In an alternative embodiment, more or fewer logics may be used to determine a dominant axis. One embodiment of implementing dominant axis assignment may be found in U.S. Ser. No. 11/603,472, now issued as U.S. Pat. No. 7,457,719 which is incorporated herein by reference. Alternative means of identifying a dominant axis may be used in other embodiments.

In one embodiment, the dominant axis logic 127 is used to determine an orientation of the electronic device 100 and/or an inertial sensor within the electronic device 100. In alternative embodiments, other logics may be used to determine an orientation of the electronic device 100.

Referring to FIG. 1, the cadence logic 132 may determine one or more sample periods to be used by the rolling average logic 135, and may determine a cadence window 150 to be used by the step counting logic 130. In one embodiment, the cadence logic 132 detects a period and/or cadence of a motion cycle. The period and/or cadence of the motion cycle may be based upon user activity (e.g. rollerblading, biking, running, walking, etc.).

Many types of motions that are useful to keep track of have a periodic set of movements. Specific periodic human motions may be characteristic of different types of user activity. For example, to walk, an individual must lift a first leg, move it forward, plant it, then repeat the same series of motions with a second leg. In contrast, a person rollerblading performs a repeated sequence of pushing, coasting and liftoff for each leg. For a particular individual, the series of walking motions will usually occur in about the same amount of time, and the series of rollerblading motions will usually occur in the same amount of time. The repeated set of motions can be considered a unit, and defines the motion cycle. The amount of time that it takes to complete one motion cycle defines the motion cycle's period, and the number of motion cycles that occur in a given unit of time define the motion cycle's cadence. For simplicity, the term "step" is used in this application to describe the user activity being evaluated. However, in the context of this application, the term "step" should be taken to mean any user activity having a periodic set of repeated movements.

FIG. 2 illustrates an exemplary motion cycle graph 200 that measures time versus acceleration, in accordance with one embodiment of the present invention. The exemplary motion-cycle graph 200 shows acceleration data taken with a single tri-axis inertial sensor. The acceleration at a given time is represented for a first axis 203, a second axis 205, and a third axis 207. In one embodiment, the cadence logic 132 of FIG. 1 analyzes the acceleration along the first axis 203, second axis 205 and third axis 207 to detect a motion cycle. Once a motion cycle is detected, a period of the motion cycle is determined, and a cadence of the motion cycle is determined. FIG. 2 shows an exemplary period of a motion cycle 210 for the third axis 207, the period 215 being approximately 0.6 seconds. The same period can also be seen to a lesser degree in the second axis 205 and the first axis 203. The corresponding cadence to the motion cycle is approximately one hundred motion cycles per minute.

In one embodiment, once a stepping period (or other motion cycle period) is determined, that period may be used to set the cadence window (the allowable time window for steps to occur). In one embodiment, the period is updated after each step. The current stepping period may be a rolling

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average of the stepping periods over previous steps, as discussed in more detail with reference to the rolling average logic 135 of FIG. 1.

A cadence window may be used to facilitate accurate measurement of a step, or other periodic human motion. A cadence window is a window of time since a last step was counted that is looked at to detect a new step. A cadence window may be set based on the period and/or cadence of the actual motion cycle (e.g., a stepping period), on set limits, and/or on other determiners.

Referring to FIG. 2, an exemplary first cadence window 240 and second cadence window 255 are shown. The first cadence window 240 may be defined by a first cadence window minimum 230 and a first cadence window maximum 235. The second cadence window 255 may be defined by a second cadence window minimum 245 and a second cadence window maximum 250. In one embodiment, the cadence window minimums 230 and 245 and cadence window maximums 235 and 250 are determined by measuring lengths of time since the most recent step was counted. In one embodiment, this length of time is measured via the timer 170 of FIG. 1. In other embodiments, other variables may be used to set the cadence window. For example, cadence windows may be determined by measuring cumulative amounts of acceleration that have been measured since the previous step was counted.

Returning to FIG. 2, cadence windows may be used to count steps until an expected step is not encountered. In one embodiment, new cadence windows are determined periodically. In one embodiment, the cadence window is a dynamic cadence window that continuously updates as a user's cadence changes. For example, using a dynamic cadence window, a new cadence window length may be set after each step. The cadence window minimums may be determined by subtracting a value from the stepping period, and the cadence window maximums may be determined by adding a value to the stepping period. In one embodiment, the cadence window maximums are preset, and the cadence window minimums are updated after each step is counted. In one embodiment, the cadence window minimums are preset, and the cadence window maximums are updated after each step is counted. In one embodiment, both the cadence window minimums and cadence window maximums are updated when a step is counted. In one embodiment, the current cadence window minimum is determined by subtracting 200 ms from the current stepping cadence period. In one embodiment, the cadence window minimum has a minimum value of 240 ms.

In the illustrated embodiment of FIG. 2, a first step 217 is counted at 0.65 seconds, and a second step 232 is counted at approximately 1.15 seconds. The first cadence window 240 opens at approximately 0.4 seconds from the first step 217, and closes at approximately 0.8 seconds from the first step 217. As shown, the second step 232 falls within the first dynamic cadence window 240. A third step 233 falls within the second dynamic cadence window 255, which may have a second cadence window minimum 245 and second cadence window maximum 250 that are different from the first cadence window minimum 230 and first cadence window maximum 235. The illustrated second cadence window minimum is about 0.35 seconds from the second step 232, and the second cadence window maximum 250 is about 0.75 seconds from the second step 232. Other cadence window minimums and maximums are also possible. When motion criteria (e.g., threshold conditions) are met within a cadence window, a step is detected, whereas when motion criteria are met outside of the cadence windows no step is detected.

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If no previous steps have been detected, there is no cadence minimum, and a step may be detected at any time that motion criteria are met. If fewer than the required number of steps to determine a dynamic cadence window have been detected, then the cadence window may have a default minimum and maximum value. In one embodiment, the cadence window has a default minimum of around 325 ms and a default maximum of around 1000 ms. Once enough steps have been detected to determine a dynamic stepping cadence or period, the cadence window may be set to the determined stepping period plus or minus an error factor. In one embodiment, a count of between about two to about ten periodic human motions is sufficient to set a dynamic cadence window.

The cadence of any periodic human motion will generally not change more than a certain amount in a given time period. In one embodiment, the cadence window may be sufficiently wide to continue counting periodic human motions even when a stepping cadence changes. In one embodiment, the cadence window is narrower, and steps may not be counted when a stepping cadence changes. So as not to miss steps, once a new stepping cadence is detected, previous measurements may be examined to determine whether they register as steps under the new stepping cadence and a new cadence window. Therefore, steps may be counted even if they did not occur in the original cadence window. The cadence window may update dynamically to a user's actual cadence. Human cadences change within a known window of rates, and so steps can be differentiated from other noise. This may ameliorate and/or eliminate missed step counts due to changes in cadence.

In one embodiment, when steps repeatedly occur at a time different from the current stepping period, a new stepping period and a new cadence window are set. For example, when the stepping period is 0.7 seconds, and a step occurs about every 0.6 seconds enough times in a row, then the stepping period is changed to 0.6 seconds and a new cadence window is set based on the changed stepping period.

Returning to FIG. 1, once the stepping period is detected, the cadence logic 132 may set one or more sample periods for the rolling average logic 135 to use based upon the stepping period. In one embodiment, the sample period(s) are set such that at least one sample period is approximately the length of, or longer than, the stepping period. In one embodiment, a sample period is set such that it is a multiple of the stepping period.

The rolling average logic 135 creates one or more rolling averages of accelerations as measured by the inertial sensor(s) over the sample period(s) set by the cadence logic 132. The rolling averages of accelerations may be used for determining an orientation of the electronic device, for determining thresholds to compare acceleration measurements against, and/or for other purposes. In one embodiment, the rolling average logic 135 creates a rolling average of accelerations for determining an orientation of the electronic device 100, the rolling average having a period that is at least the stepping period. In one embodiment, the rolling average logic creates a rolling average of accelerations for determining a lower threshold to compare acceleration measurements against, the rolling average having a sample period that is at least twice the stepping period.

The rolling average logic 135 may create one or more rolling averages of data other than accelerations. In one embodiment, the rolling average logic 135 creates a rolling average of stepping periods, where the rolling average is the rolling average time between steps. In one embodiment, the rolling average of stepping periods is calculated over the past four counted steps. The rolling average of the stepping peri-

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ods may be used by the cadence logic 132 to determine a cadence window and a current stepping cadence.

In one embodiment, rolling averages may be maintained in registries that keep track of rolling average values and the number of samples that were used to calculate current rolling average values. When a new measurement is taken, it can be incorporated into the previous rolling average value, and the registry can then be updated with a new rolling average value. Alternatively, the rolling averages may be maintained by buffering the measurements used to calculate the rolling averages. As the buffers fill, oldest measurement data can be discarded and replaced by new measurement data. The measurements in the buffer can be averaged after each measurement to determine a new rolling average.

In one embodiment, the dominant axis setting logic 140 determines an orientation of the electronic device 100 and/or the inertial sensor(s) within the electronic device 100. The orientation may be determined based upon the rolling averages of accelerations created by the rolling average logic 135. In one embodiment, once the orientation is determined, a dominant axis is assigned based upon the orientation. Determining an orientation of the electronic device 100 may include identifying a gravitational influence. The axis with the largest absolute rolling average may be the axis most influenced by gravity, which may change over time (e.g. as the electronic device is rotated). Therefore, a new dominant axis may be assigned when the orientation of the electronic device 100 and/or the inertial sensor(s) attached to or embedded in the electronic device 100 changes.

In one embodiment, the actual axis with the largest absolute rolling average over the sample period is assigned as the dominant axis. In alternative embodiments, the dominant axis does not correspond to one of the actual axes of the inertial sensor(s) in a current orientation, but rather to an axis that is defined as approximately aligned to gravity. In one embodiment, the dominant axis corresponds to a virtual axis that is a component of a virtual coordinate system. In one embodiment, the dominant axis setting logic 140 assigns the dominant axis by performing a true gravity assessment, such as by doing trigonometric calculations on the actual axes based on the gravitational influence. In one embodiment, the dominant axis setting logic 140 assigns the dominant axis by comparing the gravitational influence to a data structure such as a lookup table, associative array, hash table, adjacency matrix, etc.

Returning to FIG. 1, the step counting logic 130 may include a measurement selection logic 145, a cadence window 150, a measurement comparator 155, a threshold comparator 160, a step count buffer 165, and a mode logic 190. The measurement selection logic 145 may determine which measurements to use to determine if a step has occurred. In one embodiment, the measurement selection logic 145 may monitor accelerations relative to the dominant axis, and select only those measurements with specific relations to the dominant axis for measurement. For example, only accelerations that are approximately parallel to the dominant axis may be selected, or alternatively, only accelerations that are approximately perpendicular to the dominant axis may be selected. In one embodiment, the measurement selection logic 145 selects only measurements of acceleration data along the dominant axis. In alternative embodiments, measurements of acceleration data along other axes may also be used. In one embodiment, measurements of acceleration along only the other axes are used.

Selected measurements may be forwarded to the measurement comparator 155 and the threshold comparator 160 to determine whether a step has occurred. The measurement comparator 155 may compare a current measurement to pre-

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vious measurements. Based on this comparison, a current measurement may qualify as a step if it has met certain comparison criteria, as discussed in more detail with reference to FIG. 8.

In one embodiment, a motion cycle graph is maintained, and the current measurement is compared to the motion cycle graph. If the motion cycle graph indicates that the current measurement in relation to preceding measurements fits the profile of a step, then a step may be counted. Otherwise a step may not be counted.

Returning to FIG. 1, the threshold comparator 160 disqualifies measurements from being counted as steps for failure to meet certain thresholds. In one embodiment, measurements must be larger than a lower threshold to qualify as a step. In one embodiment, the threshold comparator 160 compares measurements to an upper threshold. In one embodiment, only a measurement having a smaller absolute value of acceleration than the upper threshold and a higher absolute value than the lower threshold is counted as a step. The upper threshold and the lower threshold are discussed in more detail below with reference to FIG. 8.

In one embodiment, the threshold comparator 160 and the measurement comparator 155 are combined into a single comparator. In one embodiment, other comparators may be used, such as a curve fitting comparator or a slope comparator.

The step count buffer 165 keeps track of probable steps. The exact behavior of the step count buffer 165 depends on which operating mode the electronic device 100 is in. In one embodiment, the operating mode that the electronic device is in is determined by the mode logic 190. In the illustrated embodiment, the mode logic 190 is a component of the step counting logic 130. In an alternative embodiment, the mode logic 190 is a separate logic from the step counting logic 130. In one embodiment, operating modes include a non-active mode, in which periodic human motions are buffered, and an active mode, in which periodic human motions are counted. In one embodiment, operating modes include a sleep mode, a step counting mode, an entry mode, and an exit mode. Operating modes are discussed in greater detail below in reference to FIG. 3.

Returning to FIG. 1, when the threshold comparator 160 and measurement comparator 155 both indicate that a measurement is a step, then the step count buffer 165 is incremented by one. Depending on the mode, when the step count buffer 165 reaches a certain amount, the step count buffer 165 is emptied and the final count 175 is incremented by the amount of steps that were in the step count buffer 165. The number of steps that must be counted by the step count buffer 165 before they register as actual steps may vary from one to ten or more, depending on the current operating mode. The final step count 175 keeps track of the total number of steps that have occurred. In one embodiment, this data is transmitted to a server or remote database.

FIG. 3 shows a state diagram for the behavior 300 of a system for monitoring human activity, in accordance with one embodiment of the present invention. The system may have multiple operating modes (states) that are navigated between by processing logic that may comprise hardware (e.g., circuitry, dedicated logic, programmable logic, microcode, etc.), software (such as instructions run on a processing device), or a combination thereof. In one embodiment, behavior 300 is the behavior of the electronic device 100 of FIG. 1.

The behavior 300 may include four operating modes for monitoring human activity: a sleep mode, an entry mode, a stepping mode, and an exit mode. In alternative embodiments, a different number of modes may be used. In one embodiment, only two modes are used: active mode and

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non-active mode. The active mode is entered once continuous steps within the cadence window have been identified, while the non-active mode is used for all other states. In alternative embodiments, multiple inactive modes and/or active modes are used. To navigate between modes, certain conditions must be met. The conditions may include exit conditions for terminating an active mode and entry conditions for initiating inactive modes. Each mode may have different exit and entry conditions.

Use of different conditions for different operating modes increases the reliability of the device that is monitoring the human activity. For example, once an object (e.g., a person) is moving, they are more likely to remain moving than to stop. Likewise, if a person is not moving, they are more likely not to move than to begin moving. These principles can be applied by requiring more stringent conditions to be met for a device to initiate a walking (stepping) mode than to continue the walking mode. The different modes may each have rules that reflect what is more likely to happen for subsequent measurements. This may reduce or eliminate the number of uncounted steps and/or false step counts.

Referring to FIG. 3, modes 300 in one embodiment include a sleep mode 305, an entry mode 315, a stepping mode 325, and an exit mode 335. In one embodiment, the power level of the system or device is linked to these modes.

The first mode initiated is the sleep mode 305. When no activity (acceleration) is detected, the system remains in sleep mode 305. When acceleration is detected, an entry mode 315 is initiated.

Once in entry mode 315, acceleration may be monitored to detect steps. When N steps are detected in appropriate cadence windows, a stepping mode 325 is initiated. If N steps are not detected within a period of time, sleep mode is reinitiated. In one embodiment, sleep mode is only initiated if no motion is detected.

Once in stepping mode 325, acceleration data is monitored to count steps according to a predefined set of rules or motion criteria. According to one of these criteria, steps are expected to occur within a set interval (e.g., within a cadence window). When a step is counted within the set interval, then the stepping mode 325 is continued. When a step is not detected within the set interval, an expected step has not occurred, and an exit mode 335 is initiated.

In exit mode 335, processing logic determines whether a predetermined number of steps (X) are detected at a particular cadence. The predetermined number of steps X may be the same as, or different from, the number of steps N. When X steps are detected in a cadence, stepping mode 325 is reinitiated. When X steps are not detected within a period of time, entry mode 315 is reinitiated.

FIG. 4 illustrates a flow diagram for a method 400 of operating an electronic device in sleep mode, in accordance with one embodiment of the present invention. In one embodiment, method 400 corresponds to the sleep mode 305 of FIG. 3. In one embodiment, the method 400 may begin when no relevant acceleration has been detected for a predetermined time interval, or when no steps have been detected for a predetermined time interval. In one embodiment, when no acceleration above a threshold value is detected for a set period of time, the sleep function is initiated. In another embodiment, when a motion signature indicative of an activity that does not need to be monitored is detected, the sleep function is initiated. For example, when the motion signature of driving is detected, the sleep function may be initiated. The time period that elapses before the sleep mode is initiated may be a fixed value, or it may be adjusted automatically by processing logic or based on user input (e.g. in response to a

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user selection of desired battery longevity verses desired performance, or based on the last measured cadence window).

Referring to FIG. 4, method 400 begins with setting a sleep mode sampling rate (block 405). In one embodiment, a low sampling rate is set. This reduces power consumption and prolongs battery life. In one embodiment, the sleep mode sampling rate is a fixed value. In alternative embodiments, the sleep mode sampling rate can be modified automatically by processing logic based on certain criteria such as time of day, user behavior patterns, etc., or based on user input.

In one embodiment, a sampling function is periodically executed in sleep mode, wherein the sampling function samples acceleration data at a set sampling rate for a set time period. For example, the sampling function may be executed every ten seconds for a duration of one second, and a sampling rate of fifty measurements per second may be set for that one second of operation. In one embodiment, the sampling function repeats at a relatively slow rate (e.g., once every 10 seconds), and the sampling rate within the sampling function is relatively high (e.g., 50 Hz). The sampling function may be used to detect unwanted motion signatures, or to maintain a device in low power sleep mode, for example, while a user is driving in a car.

In one embodiment, the sleep mode sampling rate is set to zero. The sleep mode may be set to zero, for example, when an inertial sensor has 'inertial wakeup' functionality. Inertial wakeup functionality enables processing logic to switch from sleep mode to entry mode when an acceleration exceeding a set threshold is detected. The inertial wakeup may be used to simultaneously exit sleep mode and power-up additional functionality.

At block 410, measurements of acceleration data are taken. At block 415, processing logic determines whether or not relevant acceleration is detected. Relevant acceleration includes acceleration that meets certain relevancy criteria. In one embodiment, the relevancy criteria include a lower threshold and an upper threshold. In alternative embodiments, other relevancy criteria may also be used, such as a requirement that acceleration be continuously measured for a preset time period.

When no relevant acceleration is detected, or when the 'inertial wakeup' pin has not triggered (for inertial sensors having 'inertial wakeup functionality'), sleep mode continues, and further measurements of acceleration data are taken at the set sleep mode sampling rate (block 410). When acceleration is detected, sleep mode is terminated and entry mode is initiated (block 420). In one embodiment, the acceleration that is detected and its rate of change must meet certain criteria to terminate sleep mode.

FIG. 5 illustrates a flow diagram for a method 500 of operating an electronic device in entry mode, in accordance with one embodiment of the present invention. In one embodiment, method 500 corresponds to the entry mode 315 of FIG. 3. The entry mode may be initiated when a user first begins an activity in which steps may be detected. In one embodiment, the method 500 begins when any relevant acceleration is detected. In one embodiment, entry mode is initiated when a measurement of acceleration that meets certain criteria has been detected. In one embodiment, method 500 is initiated when a sleep mode is terminated.

Referring to FIG. 5, method 500 begins by setting the sampling rate to a stepping sampling rate (block 504). The stepping sampling rate is set to facilitate accurate measurements of steps, and may be a fixed or a dynamically variable rate. A variable sampling rate may automatically adjust depending on a period of a detected stepping cadence, may be user adjusted, may adjust based on applications being run by

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processing logic, or by other means. The stepping sampling rate may be set to anywhere between about 10 and about 200 Hz. In one embodiment, the stepping sampling rate is set to about 15 to 40 Hz.

At block 510, a first step is recognized. Since no previous steps have been measured, and there is no cadence window, the first step may be recognized at any time. Once a first step is recognized, a default cadence window is set (block 514). The default cadence window may have a minimum and maximum such that steps will be counted for most or all possible stepping cadences, whether a user is walking slowly or sprinting. In one embodiment, the default cadence window has a minimum of around 325 ms and a maximum of around 1000 ms.

In one embodiment, an initial default value is set wide enough to accommodate all users, and is then dynamically adjusted to match the specific user in question. Processing logic may 'learn' (adapt to) a particular user, and may become more accurate as steps are counted. Processing logic that has the ability to learn or adapt to different users may create an individualized profile for each user. Multiple profiles may also be created for each user, the different profiles reflecting different user activity. For example, a first profile might be created for a user's running and a second profile may be created for a user's walking. Processing logic may switch between different profiles automatically, or manually based on user input. In one embodiment, processing logic compares a current cadence and/or motion cycle pattern to stored profiles. When a current cadence or motion cycle pattern matches that of a stored profile, that profile is activated.

At block 520, a buffered step count is set to one. At block 524, processing logic determines whether an additional step is recognized. An additional step may be recognized if a particular measurement of acceleration meets all the necessary criteria. One embodiment of these criteria is discussed below with reference to FIG. 8.

Returning to FIG. 5, if an additional step is recognized, method 500 continues to block 560. If no additional steps are recognized, then processing logic determines whether the time is still within the cadence window (block 530). If there is still time within the cadence window, the process returns to block 524. If the cadence window has closed, then the buffered step count is reset to zero (block 534). The process then continues to block 540.

At block 540, processing logic determines whether any relevant acceleration is detected. If no relevant acceleration is detected, then sleep mode is initiated (block 544). If some relevant acceleration is detected, then processing logic returns to block 510 to await recognition of another first step. If at block 524 an additional step was recognized, the process continues to block 560.

At block 560, an additional step is added to the buffered step count. Processing logic then checks whether there are M counts in the buffered step count (block 564). In one embodiment, M is an integer value between about 4 and 10. If there are not at least M steps in the buffered step count, then the process returns to block 524.

If the buffered step count is equal to or greater than M, then the processing logic checks whether the cadence window is set to the default (block 570). If the cadence window is still set to the default, then a new cadence window is set (block 574) based on a stepping cadence of the M steps measured. The process then returns to block 524. If the cadence window is not set to the default, then processing logic continues to block 580. In an alternative embodiment, once there are M steps in the buffered step count, the cadence window may be adjusted for each additional step that is recognized.

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At block **580**, processing logic checks whether there are N steps in the buffered step count (block **580**), where N may be an integer value greater than M. When there are not yet N steps in the buffered step count, the process returns to block **524** to continue in entry mode. When the number of steps in the buffered step count reaches N, the buffered steps are added to an actual or final step count, and a stepping mode is entered into (block **584**).

FIG. **6** illustrates a flow diagram for a method **600** of operating an electronic device in stepping mode, in accordance with one embodiment of the present invention. In one embodiment, method **600** corresponds to the stepping mode **325** of FIG. **3**. The stepping mode may be initiated when a user has been walking long enough for a buffered step count to fill. In one embodiment, method **600** is initiated when an entry mode is terminated, and/or when an exit mode is terminated.

Referring to FIG. **6**, method **600** begins by setting a cadence window (block **610**). The cadence window may be set based on previous measurement data. In one embodiment, the cadence window is set based on a rolling average of stepping periods. In one embodiment, the cadence window may be identical to the cadence window used during entry mode. Once the cadence window is set, measurement data is checked to determine whether an additional step is recognized (block **615**). If an additional step is recognized, then it is added to the final or actual step count (block **620**). If no additional step is recognized, then processing logic determines whether the current measurement was taken within the cadence window (block **625**). If the cadence window has not elapsed, the process returns to block **615**. If the cadence window has elapsed, then an expected step was not counted, and an exit mode is initiated (block **630**).

FIG. **7** illustrates a flow diagram for a method **700** of operating an electronic device in exit mode, in accordance with one embodiment of the present invention. In one embodiment, method **700** corresponds to the exit mode **335** of FIG. **3**. The exit mode may be entered into when an expected step is not identified in stepping mode.

In one embodiment, the requirement(s) for changing from exit mode to stepping mode are less strict than the requirement(s) for switching from entry mode to stepping mode. Processing logic may assume that when a user has recently taken a step, the user is most likely to take another step. Processing logic may also assume that if a user has not just taken a step, it is most likely that they will not take one. These assumptions may be implemented by imposing more stringent requirements to switch from entry mode to stepping mode than to change from exit mode to stepping mode.

An expected step may not be identified, for example, when a user stops walking, when extraneous movements such as gestures are made that interfere with the step count, or when a device orientation is changed as a step occurs. In one embodiment, the exit mode assumes that a step has been missed, so that if the exit mode determines that a user is still walking, the originally uncounted step is not missed.

The process begins by initiating a step timer (block **705**). The step timer measures the amount of time that has passed since a step has been identified. In one embodiment, the step timer is a countdown timer that terminates exit mode when the timer reaches zero. In one embodiment, the step timer starts counting when a cadence window minimum is reached, and stops counting when a cadence window maximum is reached. In an alternative embodiment, the step timer starts counting as soon as the exit mode is initiated, and stops counting when a cadence window maximum is reached. In

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one embodiment, the step timer starts counting at 240 ms from the time that the expected step should have occurred.

At block **710**, a step is added to a buffered step count. At block **715**, processing logic determines whether the buffered step count is equal to X, where X is the number of identified steps in exit mode. In one embodiment, X is between 3 and 8. If the buffered step count is equal to X, then the buffered steps are added to the actual step count and stepping mode is reinitiated (block **720**). If the buffered step count is not equal to X, then processing logic proceeds to block **725**.

At block **725**, processing logic determines whether the step timer has timed out (allotted time has elapsed). In one embodiment, the step timer times out when no steps are counted within a cadence window. In one embodiment, the step timer times out when no steps are counted in two or more cadence windows. If the allotted time has elapsed, then the buffered step count is cleared, and entry mode is initiated (block **730**). If the allotted time has not elapsed, then processing logic determines whether an additional step is recognized (block **735**). If a step is recognized, then the step timer is reset (block **705**), the buffered step count is incremented by one (block **710**), and on the process continues to block **715**. If a step is not recognized, then processing logic returns to block **725** to determine whether the step timer has elapsed. In an alternative embodiment, the step timer is not reset when an additional step is recognized, and the buffered step count must reach X in the time initially allotted by the step timer. In that instance, the step timer is set at greater than X times the cadence window.

FIG. **8** illustrates a flow diagram for a method **800** of recognizing a step, in accordance with one embodiment of the present invention. In one embodiment, method **800** may be executed by blocks **510** and **524** of FIG. **5**, block **615** of FIG. **6** and block **735** of FIG. **7**. In one embodiment, method **800** is performed by electronic device **100** of FIG. **1**.

Referring to FIG. **8**, method **800** begins with measurements of acceleration data being taken (block **805**). Measurements are taken according to a sampling rate, which may vary from about one measurement per second to many measurements a second, depending on the operating mode being used.

At processing block **810**, in one embodiment measurements are filtered. Measurements can be filtered to remove high frequency data and/or low frequency data. In one embodiment, what data to filter depends on the type of user activity detected. At processing block **812**, in one embodiment the inertial sensor is oriented by assigning a dominant axis. Assigning a dominant axis may include calculating rolling averages of acceleration and assigning the dominant axis based on the rolling averages of acceleration.

At block **815**, processing logic determines whether a measurement is within a cadence window. If the measurement is not within a cadence window, then no step may be recognized or counted for that measurement (block **840**). If the measurement is within the cadence window, the process continues to block **820**.

At block **820**, processing logic determines whether acceleration along the dominant axis is greater than a lower threshold. If the measurement is not greater than the lower threshold, no step may be recognized or counted for that measurement (block **840**). If the measurement is greater than the lower threshold, the processing logic continues to block **825**.

In one embodiment, the measurement may qualify as a step if it is the first measurement that crosses the lower threshold. In an alternative embodiment, the measurement with the greatest acceleration within a cadence window (e.g. a peak) may be counted as a step.

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The lower threshold may be based on a rolling average of accelerations as determined by the rolling average logic 135 of FIG. 1. In one embodiment, the rolling average of accelerations that is used to set the lower threshold has a sample period that is about twice the stepping period. In alternative

embodiments, other sample periods are used for the rolling average. In one embodiment, the lower threshold is set such that an absolute value of a measurement must exceed an absolute value of the rolling average to be counted as a step. Multiple lower thresholds may be set, and a current measurement may be compared to one or more of the lower thresholds depending on operating conditions. For example, a negative lower threshold may be used if acceleration is detected in a negative direction (e.g., when device is upside down), and a positive lower threshold may be used if acceleration is detected in a positive direction (e.g., device is right-side up). In one embodiment, absolute values may be used.

In one embodiment, the measurement must exceed the rolling average by a set margin. The margin may be set automatically by processing logic, or it may vary based on the orientation of the electronic device or inertial sensor(s), user input, and/or other criteria.

In one embodiment, the lower threshold is adjusted based on an orientation of the electronic device and/or an orientation of the inertial sensor(s) within the electronic device. If an axis is closely aligned with gravity, a first threshold may be used. If no axes are closely aligned to gravity, other thresholds may be used. In one embodiment, a variable threshold is used, the variable threshold having a larger value when an axis is closely aligned to gravity, and progressively lower values as an axis most closely aligned with gravity is moved out of line with gravity. The variable threshold can be implemented using a data structure (e.g., a lookup table, hash table, adjacency matrix, etc.), comparison to a virtual axis, or by performing trigonometric calculations.

At block 825, processing logic determines whether acceleration along the dominant axis is greater than previous measurements. In one embodiment, acceleration along the dominant axis for a present measurement is compared to the previous 1 to 4 measurements.

In one embodiment, the absolute value of the present measurement is compared to the absolute value of the previous measurement or measurements. By comparing the absolute value of acceleration along the dominant axis to previous absolute value(s) of acceleration, processing logic may determine whether the acceleration of a user is moving away from the influence of gravity (e.g. whether a person is lifting a foot from the ground rather than planting it on the ground). In one embodiment, a measurement qualifies as a step when it reflects that the acceleration of a user is moving away from gravity. Alternatively, a current measurement may qualify as a step if it has an absolute value that is less than absolute values of the previous measurements, indicating that the acceleration of a user is moving towards gravity.

If the absolute value of the current measurement is not greater than the absolute values of the measurements compared to, then no step may be recognized or counted for that measurement (block 840). If the absolute value of the measurement is greater than the absolute values of previous measurements, then the process continues to block 830.

At block 830, processing logic determines whether acceleration for a particular measurement is lower than an upper threshold. In one embodiment, only acceleration along the dominant axis is compared to the upper threshold. In one embodiment, accelerations along all axes are compared to the upper threshold. If the current measurement is not lower than

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the upper threshold, then no step may be recognized or counted for that measurement (block 840). If the measurement is lower than the upper threshold, then a step may be counted (block 835). The upper threshold may be set to prevent sudden accelerations such as taps from being counted as steps.

Blocks 815, 820, 825 and 830 show four criteria that may be used to accurately determine whether user has walked or run one step. These criteria may be dynamic motion criteria that are updated continuously as current conditions change (e.g., as an inertial sensor changes orientation, as a user changes cadence, etc.). Alternatively, these criteria may be static criteria that are preset, or criteria that may be changed through user input.

As noted above, though embodiments of the present invention are described in reference to steps, the present invention equally applies to other periodic human motions. Other criteria may also be used in addition to, or in place of, those listed above. These criteria may reduce or eliminate the number of false steps counted and/or the number of missed steps. Examples of other criteria include specific rates of change in acceleration between measurements, specific shapes and/or sharpness of acceleration peaks for motion cycles, particular amplitudes of periodic human motions, etc. These and other criteria may be applied to embodiments of the present invention.

FIG. 9 illustrates a flow diagram for one embodiment of a method 900 of orienting an inertial sensor. In one embodiment, the method 900 is executed by block 812 of FIG. 8.

Referring to FIG. 9, method 900 begins with detecting a stepping period (block 910). In one embodiment, the method 900 may begin by detecting a stepping cadence. At block 915, rolling averages of accelerations are created. The rolling averages of accelerations may be created based on the stepping period (or stepping cadence). In one embodiment, multiple rolling averages of accelerations are created.

At block 920, a dominant axis is assigned. In one embodiment, the dominant axis is assigned after identifying a gravitational influence. The gravitational influence may be identified by calculating total acceleration based upon the acceleration on each axis. In one embodiment, the percentage of the total acceleration can then be assigned to each axis and an approximate device orientation can be determined.

In the foregoing description, numerous specific details have been set forth such as examples of specific systems, languages, components, etc. in order to provide a thorough understanding of the present invention. It will be apparent, however, to one skilled in the art that these specific details need not be employed to practice the present invention. In other instances, well known materials or methods have not been described in detail in order to avoid unnecessarily obscuring the present invention.

The present invention may be performed by hardware components or may be embodied in machine-executable instructions, which may be used to cause a general-purpose or special-purpose processor programmed with the instructions to perform the method described above. Alternatively, the method may be performed by a combination of hardware and software.

The present invention may be provided as a computer program product, or software, that may include a machine-readable medium having stored thereon instructions, which may be used to program a computer system (or other electronic devices) to perform a process according to the present invention. The machine-readable medium may include, but is not limited to, floppy diskettes, optical disks, CD-ROMs, and magneto-optical disks, ROMs, RAMs, EPROMs,

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EEPROMs, magnetic or optical cards, flash memory, or other type of media or machine-readable mediums suitable for storing electronic instructions.

In the foregoing specification, the invention has been described with reference to specific exemplary embodiments thereof. It will, however, be evident that various modifications and changes may be made thereto without departing from the broader spirit and scope of the invention as set forth in the appended claims. The specification and drawings are, accordingly, to be regarded in an illustrative rather than a restrictive sense.

What is claimed is:

1. A method of monitoring human activity using an inertial sensor, comprising:

assigning a dominant axis with respect to gravity based on an orientation of the inertial sensor;

detecting a change in the orientation of the inertial sensor and updating the dominant axis based on the change; and counting periodic human motions by monitoring accelerations relative to the dominant axis by counting the periodic human motions when accelerations showing a motion cycle that meets motion criteria is detected within a cadence window; and

updating the cadence window as actual cadence changes.

2. The method of claim 1, further comprising:

using acceleration measurements along only the dominant axis to count steps.

3. The method of claim 1, wherein at least one of the motion criteria is a dynamic motion criterion, the dynamic motion criterion updated to reflect current conditions.

4. The method of claim 3, wherein the dynamic motion criteria includes at least a lower threshold, wherein the lower threshold is adjusted based on at least one of a rolling average of accelerations and the orientation of the inertial sensor.

5. A method of monitoring human activity using an inertial sensor, comprising:

buffering a plurality of periodic human motions, each periodic human motion comprising a motion cycle;

identifying a number of periodic human motions within an appropriate cadence window;

counting each of the periodic human motions to enable the monitoring of human activity; and

updating the cadence window as a cadence of the motion cycle changes.

6. The method of claim 5, further comprising:

switching the device from the active mode to the non-active mode when a number of expected periodic human motions are not identified in the appropriate cadence windows.

7. The method of claim 5, further comprising:

switching from a sleep mode to the non-active mode of operation when an acceleration is detected.

8. The method of claim 5, wherein prior to identifying, the inertial sensor is in a non-active mode, and wherein the non-active mode comprises running the device in one of an exit mode and an entry mode.

9. The method of claim 8, wherein:

a requirement for switching the device from the exit mode to an active mode is lower than a requirement for switching the device from the entry mode to the active mode.

10. An inertial sensor based device, comprising:

a dominant axis logic to determine an orientation of a device with respect to gravity, to assign a dominant axis, and to update the dominant axis when the orientation of the device changes; and

a counting logic to count periodic human motions by monitoring accelerations relative to the dominant axis by

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counting the periodic human motions when accelerations showing a motion cycle that meets motion criteria is detected within a cadence window; and

a cadence logic to update the cadence window as actual cadence changes.

11. The device of claim 10, wherein:

the counting logic uses acceleration measurements along only the dominant axis to count steps.

12. The device of claim 10, further comprising:

the cadence logic to update a dynamic cadence window; and

the counting logic to count a periodic human motion when an acceleration measurement that meets motion criteria is taken within the cadence window.

13. The device of claim 10, further comprising:

a comparator, to compare measurements of acceleration to dynamic motion criteria, the dynamic motion criteria updated to reflect current conditions; and

the counting logic to count a periodic human motion when the measurements of acceleration satisfy the dynamic motion criteria.

14. A non-transitory machine readable medium containing executable computer program instructions which, when executed by a processing system, cause said system to perform a method for:

assigning a dominant axis with respect to gravity based on an orientation of the inertial sensor;

detecting a change in the orientation of the inertial sensor and update the dominant axis based on the change; and counting periodic human motions by monitoring accelerations relative to the dominant axis by counting the periodic human motions when accelerations showing a motion cycle that meets motion criteria is detected within a cadence window; and

updating the cadence window as actual cadence changes.

15. The non-transitory machine readable medium containing executable computer program instructions of claim 14, which, when executed by the processing system, cause said system to perform the method further for:

using acceleration measurements along only the dominant axis to count steps.

16. The non-transitory machine readable medium containing executable computer program instructions of claim 14, which, when executed by the processing system, cause said system to perform the method further for:

switching the device from an active mode to a non-active mode when a number of expected periodic human motions are not identified in the appropriate cadence windows.

17. The non-transitory machine readable medium containing executable computer program instructions of claim 14, which, when executed by the processing system, cause said system to perform the method further for:

maintaining a cadence window, wherein the cadence window is updated as an actual cadence changes; and counting a periodic human motion when an acceleration measurement that meets motion criteria is within the cadence window.

18. The non-transitory machine readable medium containing executable computer program instructions of claim 17, wherein at least one of the motion criteria is a dynamic motion criterion, the dynamic motion criterion updated to reflect current conditions.

19. The non-transitory machine readable medium containing executable computer program instructions of claim 14, wherein the dynamic motion criteria includes at least a lower

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threshold, wherein the lower threshold is adjusted based on at least one of a rolling average of accelerations and the orientation of the inertial sensor.

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